In the Claims:

Kindly rewrite the claims as follows:

- 1. (Currently amended) A method of measuring the a_QT interval of an electrocardiogram (ECG) signal wherein the an end of the a_T wave is identified from ECG data, the end of the T wave being determined by reference to the timing of at least one intersection at which an upright T wave of a first set of derived ECG signal data intersects an inverted T wave of a second set of derived ECG signal data, the two sets of ECG data being superimposed so as to maximize their data fit over a segment of the ECG signal after a peak of the positive T wave peak.
- 2. (Currently amended) A The method as claimed in claim 1 wherein the data fit of said data is maximised by a least squares calculation.
- 3. (Currently amended) A-The method as claimed in claim 1 or 2, wherein the method comprises the steps of:
 - (a) acquiring ECG signal data;
 - (b) deriving a first set of reduced noise ECG signal data from the acquired ECG signal data;
 - (c) inverting the first reduced noise set of reduced noise ECG signal data to derive an inverted set of reduced noise ECG signal data;
 - (d) identifying a portion of each set of ECG signal data corresponding to a said segment after the T wave;
 - (e) calculating an offset such as to fit the first set of data to the inverted set of data over said segment;
 - (f) detecting at least one intersection between the first set of data and the inverted set of data by reference to said offset; and
 - (g) determining the an end of said QT intervals interval by reference to the timing of the detected intersection(s).

- 4. (Currently amended) A-The method as claimed in claims claim 3 wherein in step (g) the end of the QT interval is determined by the a first point intersection.
- 5. (Currently amended) A The method as claimed in any previous claim 4 wherein the end of the T wave is defined at the first point of intersection in said segment, provided there is at least one other point of intersection after a predetermined interval.
- 6. (Currently amended) A The method as claimed in any previous claim 1 wherein said interval can be varied according to the noise content in the a segment of the an ECG deemed to be the an isoelectric line baseline segment.
- 7. (Currently amended) A The method as claimed in any of claims claim 3 to 6 wherein the step (b) comprises calculating the a median signal for each time from an ensemble of ECG signals for each lead to reduce low frequency baseline noise.
- 8. (Currently amended) A-The method as claimed in any of claims 3 to claim 7 wherein the method step (b) further comprises smoothing the median ensembled ECG signal with a moving median filter to reduce high frequency noise.
- 9. (Currently amended) A-The method as claimed in any of claims 3 to claim 8 wherein the method step (b) further comprises filtering the median smoothed, median ensembled ECG signal using a wavelet frequency thresholding technique which substracts the magnitudes of any non-zero frequency components within the isoelectric baseline segment from the rest of the ECG thus further de-noising it.
- 10. (Currently amended) A-The method as claimed in any of claims 3 to claim 9 wherein the step (b) further includes vertically shifting the smoothed median ensembled ECG-signal so that the a minimum value after peak of T is zero.

- 11. (Currently amended) A-The method as claimed in any of claims 3 to claim 10 wherein the step (b) further comprises the steps of detecting and correcting baseline drift in the first set of ECG data.
- 12. (Currently amended) A-The method as claimed in any preceding claim 11 wherein the detecting step-includes the testing for the presence of a single crossing of one isoelectric line.
- 13. (Currently amended) A-The method as claimed in any preceding claim 12 wherein the an ensembled ECG can be is rotated about a zero point or otherwise transformed to reconfigure the set of ECG data to have multiple crossings of said line.
- 14. (Currently amended) A-The method as claimed in any of claims claim 3 to 13-wherein the step (b) further includes applying a non-linear function such as squaring the amplitudes of the signal for all time instants, in order to accentuate features of interest and ensure positive deflections of the T wave.
- 15. (Currently amended) A-The method as claimed in any of claims 3 to claim 14 wherein the step (b) further includes summing the squared amplitudes of ensembled orthogonal leads over all time instants to give a squared resultant vector ensembled ECG.
- 16. (Currently amended) A-The method as claimed in any preceding claim 1 wherein the method further includes finding the a beginning of the QT interval by an established method, for example from the median of ensembled ECG signals from all 12 leads.
- 17. (Currently amended) A-The method as claimed in any preceding claim 16 wherein the method includes calculating the QT interval by subtracting the beginning of the QT interval from the calculated end of the T wave.
- 18. (Currently amended) A-The method as claimed in any preceding-claim 1 wherein the QT interval is measured for the squared vector resultant data derived from quasi-orthogonal or actual orthogonal XYZ leads, and the a longest of QT measurements made in 3 dimensions is made.

- 19. (Currently amended) A-The method as claimed in any preceding claim 3 wherein the ECG signal data may be is acquired in step (a) from the a set of standard ECG leads including I, aVf and V2.
- 20. (Currently amended) An apparatus for measuring the QT interval of an electrocardiogram (ECG) signal wherein there is provided comprising means for identifying the an end of the a T wave from ECG data, the end of the T wave being defined as the a first time of intersection at which an upright T wave of a first set of derived ECG signal data intersects an inverted T wave of a second set of derived ECG signal data, the two sets of data being superimposed so as to maximise their data fit over a segment of the ECG signal after a peak of the positive T wave peak.
- 21. (Currently amended) An-The apparatus as claimed in claim 20 wherein the data fit of said data is maximised by a least squares calculation.
- 22. (Currently amended) An The apparatus as claimed in claim 20 or 21 wherein the apparatus comprises:

means for acquiring ECG signal data;

means for deriving a first set of reduced noise ECG signal data from the acquired ECG signal data;

means for inverting the first <u>set of reduced noise set of ECG</u> signal data to derive an inverted set of reduced noise ECG signal data;

means for identifying a portion of each set of ECG signal data corresponding to a the segment after the T-wave;

means for calculating an offset such as to fit the first set of data to the inverted set of data over said segment;

means for detecting at least one intersection between the first <u>set</u> and <u>the</u> inverted set of data by reference to said offset; and

means for determining the an end of said QT intervals interval by reference to the timing of the detected intersection(s).

- 23. (Currently amended) An-The apparatus as claimed in claim 22 wherein in the means for determining the end of said QT interval, the QT interval is determined by the a first point of intersection.
- 24. (Currently amended) An-The apparatus as claimed in claims 22 or claim 23 wherein the end of the T wave is defined at the first point of intersection in said segment, provided there is at least one other point of intersection after a predetermined interval.
- 25. (Currently amended) An The apparatus as claimed in any of claims claim 22 to 24 wherein said interval can be varied according to the noise content in the a segment of the an ECG deemed to be the isoelectric line baseline segment.
- 26. (Currently amended) An The apparatus as claimed in any of claims claim 22 to 24 wherein the means for deriving a first set of reduced noise ECG signal data comprises means for calculating the a median signal for each time from an ensemble of ECG signals for each lead to reduce low frequency baseline noise.
- 27. (Currently amended) An The apparatus as claimed in any of claims 22 to claim 26 wherein the means for deriving a first set of reduced noise ECG signal data further comprises means for smoothing the median ensembled ECG signal with a moving median filter to reduce high frequency noise.
- 28. (Currently amended) An-The apparatus as claimed in any of claims 22 to claim 27 wherein the means for deriving a first set of reduced noise ECG signal data further comprises means for filtering the median-smoothed, median ensembled signal ECG using a wavelet frequency thresholding technique which substracts the magnitudes of any non-zero frequency components within the isoelectric baseline segement segment from the a rest of the ECG thus further de-noising it.

- 29. (Currently amended) An-The apparatus as claimed in any of claims 22 to 28 claim 27 wherein the means for deriving a first set of reduced noise ECG signal data further includes means for vertically shifting the smoothed median ensembled ECG-signal so that the a minimum value after peak of T is zero.
- 30. (Currently amended) An-The apparatus as claimed in any of claims claim 22 to 29 wherein the means for deriving a first set of reduced noise ECG signal data further comprises means for detecting and correcting baseline drift in the first set of ECG data.
- 31. (Currently amended) An-The apparatus as claimed in any of claims 20 to claim 30 wherein detection the means for detecting includes means for the testing for the presence of a single crossing of one isoelectric line.
- 32. (Currently amended) An The apparatus as claimed in any of claims 20 to claim 31 wherein there is provide further comprising means for rotating the an ensembled ECG about a zero point or otherwise transformed transforming the ensembled ECG to reconfigure the set of ECG data to have multiple crossings of said line.
- 33. (Currently amended) An-The apparatus as claimed in any of claims claim 22 to 32 wherein the means for deriving a first set of reduced noise ECG signal data further includes means for applying a non-linear function such as squaring the amplitudes of the signal for all time instants, in order to accentuate features of interest and ensure positive deflections of the T wave.
- 34. (Currently amended) An The apparatus as claimed in any of claims claim 22 to 33 wherein the means for deriving a first set of reduced noise ECG signal data further includes means for summing the squared amplitudes of ensembled orthogonal leads over all time instants to give a squared resultant vector ensembled ECG.

- 35. (Currently amended) An The apparatus as claimed in any of claims claim 20 to 34 wherein the apparatus further includes means for finding the a beginning of the QT interval by an established method, for example from the median of ensembled ECG signals from all 12 leads.
- 36. (Currently amended) An The apparatus as claimed in any of claims 20 to claim 35 wherein the apparatus includes means for calculating the QT interval by subtracting the beginning of the QT interval from the calculated end of the T wave.
- 37. (Currently amended) An-The apparatus as claimed in any of claims claim 20 to 36 wherein the QT interval is measured for the squared vector resultant data derived from quasi-orthogonal or actual orthogonal XYZ leads, and the a longest of QT measurements made in 3 dimensions is made.
- 38. (Currently amended) An-The apparatus as claimed in any of claims claim 20 to 35 wherein the ECG signal data is acquired from the a set of standard ECG leads including I, aVf and V2.
- 39. (Currently amended) A record carrier wherein are comprising recorded program instructions for causing a programmable processor to perform the steps of the method as claimed in claims claim 1 to 19, or to implement an apparatus having the features claimed in any of claims 20 to 38.
- 40. (New) A record carrier comprising recorded program instructions for causing a programmable processor to implement an apparatus having the features claimed in claim 20.